Neural tube patterning: from a minimal model for rostrocaudal patterning toward an integrated 3D model

**Highlights**

- WNT regulates rostrocaudal neural tube patterning via a tristable network motif.
- Blocking hindbrain fate may improve generation of dopaminergic neurons from hPSCs.
- Combined rostrocaudal and dorsoventral model correctly patterns 3D neural tube.
- Models of in vivo processes can be built modularly using data from diverse sources.
Neural tube patterning: from a minimal model for rostrocaudal patterning toward an integrated 3D model

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SUMMARY
Rostrocaudal patterning of the neural tube is a defining event in vertebrate brain development. This process is driven by morphogen gradients which specify the fate of neural progenitor cells, leading to the partitioning of the tube. Although this is extensively studied experimentally, an integrated view of the genetic circuitry is lacking. Here, we present a minimal gene regulatory model for rostrocaudal patterning, whose tristable topology was determined in a data-driven way. Using this model, we identified the repression of hindbrain fate as promising strategy for the improvement of current protocols for the generation of dopaminergic neurons. Furthermore, we combined our model with an established minimal model for dorsoventral patterning on a realistic 3D neural tube and found that key features of neural tube patterning could be recapitulated. Doing so, we demonstrate how data and models from different sources can be combined to simulate complex in vivo processes.

INTRODUCTION
In Parkinson’s disease (PD), the dopaminergic neurons (DA) of the substantia nigra of the brain undergo pathological deterioration. The resulting deficiency in striatal dopamine leads to symptoms such as tremor, bradykinesia and rigidity that can currently not be relieved sufficiently by pharmacological treatment (Chinta and Andersen, 2005; Takagi et al., 2005). Today, transplantation therapy is the most promising approach to achieving PD recovery (Lehnen et al., 2017); several studies and clinical trials have demonstrated restoration of dopaminergic activity and partial symptom relief for up to 18 years post-transplantation (Barker et al., 2015; Kefalopoulou et al., 2014; Takagi et al., 2005). The conventional source of cells for these transplants, human fetal ventral mesencephalic tissue – which contains a high concentration of dopaminergic neuroblasts (Kefalopoulou et al., 2014; Lindvall, 2012) – is naturally scarce, ethically controversial and suffers from highly variable results (Lindvall, 2012). Recently, it has been suggested that DA progenitor generation by differentiation of human pluripotent stem cells (hPSCs) presents an alternative approach. Studies in animal models have shown that hPSC-derived DA progenitors are equivalent to fetal cells in terms of subtype specific marker expression, controlled dopamine release and functional PD symptom relief (Grealish et al., 2014; Kirkeby and Parmar, 2012a, 2012b; Kriks et al., 2011; Lehnen et al., 2017; Steinbeck et al., 2015). To date, various protocols have been developed to efficiently derive DA progenitors from human embryonic stem cells; many of them focusing on tuning a combination of WNT, SHH and FGF8 with great success (Adil et al., 2017; Cho et al., 2008; González et al., 2013; Kim et al., 2002; Kirkeby et al., 2012; Nolbrant et al., 2017). These protocols are inspired by the mechanisms and actors found in the development of the neural tube in vivo. Therefore, a better understanding of correct and reliable DA differentiation in vivo would not only shed light on the development of the early brain, but also contribute to improving current in vitro protocols for midbrain DA neuron generation.

In vivo neural patterning is a complicated and concerted process that relies on the three-dimensional diffusion of various morphogen signals in an uneven geometry. In humans, the current understanding of this process can be summarised as follows. By the end of the fourth week of embryonic development the progenitor of the embryo’s brain, the neural tube, is patterned along the rostrocaudal axis into three distinct regions that develop into forebrain, midbrain and hindbrain (Gasser, 1975). In addition, patterning occurs along the dorsoventral axis, setting up numerous progenitor cell types such as motor neurons and...
interneurons (Wilson and Maden, 2005). The formation and subdivision of the neural tube is the result of extracellular morphogens that are released in specific areas of the tube, establishing concentration gradients. The cells of the neural tube are able to interpret the local concentration of these gradients and take fate decisions accordingly. Since gene regulatory networks have been shown to control pattern formation in multiple tissues (Briscoe, 2019; Peter et al., 2012; Peter and Davidson, 2015; Sagner and Briscoe, 2017), the developing vertebrate neural tube pattern might be the response of transcriptional circuitry inside neural progenitor cells to morphogen gradients. Dorsoventral patterning is mainly controlled by opposing signaling gradients of WNT/BMP from the roof plate, and SHH from floor plate cells (Ulloa and Martí, 2009) and the zona limitans intrathalamica (Carlson, 2013). Neural tube rostrocaudal patterning is mainly governed by WNT-signalling, emerging from the isthmic organizer (Tao and Zhang, 2016) and the midbrain floor plate in the cephalic flexure (Joksimovic et al., 2009; Prakash et al., 2006). It has been shown in vitro that controlling the gradient of the WNT-signalling, using Glycogen synthase kinase 3 (GSK3) inhibitors either in different cell cultures (Kirkeby et al., 2012) or in microfluidic devices (Ríes et al., 2020a; Ríes et al., 2020b), acting on differentiating human embryonic stem cells can lead to progressive caudalisation from forebrain to hindbrain. However, the gene regulatory network acting downstream of WNT-signalling that regulates this patterning processes has not been elucidated.

In this study, we propose a minimal gene regulatory network model for rostrocaudal neural tube patterning. The transcriptional circuit topology was determined in an unbiased way and the model parameters were optimised using gene expression data from a study on hPSCs, which were cultured in conditions with varied levels of WNT-signalling (Kirkeby et al., 2012). Subsequently, model parameter sensitivity analysis revealed the key interactions that drive the patterning process. Moreover, knockdown and overexpression model simulations gave insight into the regulation of the patterning and enabled the prediction of more efficient protocols for the generation of DA neurons in vitro. Furthermore, our optimised model was combined with the model controlling dorsoventral patterning proposed in (Balaskas et al., 2012) to simulate the pattern of the neural tube in a realistic, three-dimensional (3D) geometry, since recent advances in PD research incorporating organoids (Monzel et al., 2017; Smits et al., 2019) make it necessary to not only investigate morphogen and gene interactions but also the effects of tissue geometry on neural patterning. This way, we investigated which parts of the neural tube’s pattern could be explained by our minimal 3D model. Moreover, by integrating theoretical models and quantitative data from different sources, we propose a ‘divide and conquer’ framework for the successive development of mathematical models capable to elucidate complex biological processes - for which often comprehensive datasets are not obtainable.

**RESULTS**

**Gene expression of GSK3i treated cells clusters three-fold**

As a first step toward a minimal gene regulatory network for rostrocaudal neural tube patterning, we aimed to identify the essential genes involved in this process. To this end, we used experimental data consisting of the expression levels of a selection of genes recorded in hPSCs for varying concentrations of the GSK3 inhibitor CHIR99021 (CT) obtained via quantitative PCR (qPCR). This dataset has been published in (Kirkeby et al., 2012). GSK3 is a negative regulator of canonical WNT-signalling, i.e. low GSK3 activity emulates strong WNT activity and vice versa. To identify the genes that correspond to the patterned brain regions, we determined the correlation between the gene expression across the varied CT concentrations. For this, we used a hierarchical agglomerative clustering approach, resulting in a correlation cluster map (Müllner, 2011) (Figure 1A). From this analysis, we identified the three major clusters with positive correlation. Examining the expression levels of these three gene clusters, three distinct regions of gene expression were found for varied levels of CT (Figure 1B). For the gene regulatory network model parameter and topology optimisation we selected one representative gene for each brain region. For the forebrain (FB) region we used forkhead box G1 (FoxG1), since it has been shown to be involved in telencephalon fate (Kobayashi et al., 2002; Toresson et al., 1998; Xuan et al., 1995). The midbrain (MB) region was represented by engrailed 2 (EN1), due to its key role in DA neuron specification (Alves dos Santos and Smidt, 2011; Kouwenhoven et al., 2017). For the hindbrain (HB) region we chose HOXA2, as it is reported to be a central regulator in hindbrain fate (Barrow et al., 2000; Davenne et al., 1999). The selection of one representative gene per brain region enabled us to construct a minimal gene regulatory network to capture the dynamics of neural tube patterning. However, it is important to note that this does not necessarily imply that the selected genes are interacting directly or are primarily regulating cell fate specification. Therefore, in the following results, the labels FB, MB and HB are used, when referring to the genes.
Unbiased topology selection identifies a tristable switch configuration

With the key players of the network identified, the next step toward a minimal gene regulatory network was the determination of their interactions i.e. the connection between the nodes. These nodes are FB, MB, HB, GSK3 and CT (Figure 1C). We determined the interaction between these nodes and the resulting network topology in an unbiased way by optimising all possible configurations toward the experimental data. The only two interactions that were pre-defined are the inhibition of GSK3 by CT, which resulted in the necessity of GSK3 self-activation to allow for steady state activity of GSK3. The remaining interactions could be either activation or repression, which made for 4,096 possible network configurations. The configurations that yielded the lowest cost function \( E_d \) (see STAR Methods) after parameter optimisation were considered as the optimal configurations (Figure 1D); two topologies satisfied this criterion. These two configurations only differed in the self-interaction of FB, which was activation in one case and repression in the other. However, the corresponding rate constant \( c_0 \) (see STAR Methods) had a significantly smaller value compared to the other rate constants and therefore we concluded that, for the purpose of this minimal model, FB does not self-interact.

To verify that the found topology was not specific to the selected representative genes, we optimised our model toward all remaining 759 permutations of region-specific genes (Figure S1A) and found that in the majority of cases, the model was able to recapitulate the data. Moreover, we randomly selected 16 permutations of region-specific genes and repeated the topology selection as described before, (Figure S1B). This revealed that in more than 80% of the cases (13/16) the found optimal topology was very similar or identical to the initial one. These results demonstrate that the found tristable switch topology generally captures the interaction between the region-specific genes.

The model resulting from the unbiased topology selection is shown in Figure 1E. In this model, the three brain regions are mutually repressive and hence form a tristable switch. MB and HB fate are downregulated by GSK3, whereas FB fate is positively regulated. Also, FB does not self-interact and therefore directly

Figure 1. Experimental data from in vitro neural patterning experiments and model selection

(A) Correlation cluster map of the different brain region specific genes across CT concentrations. Three clusters were identified, which correspond to the three brain regions.

(B) Normalised gene expression of FB, MB and HB specific genes for different concentrations of the GSK3 inhibitor CT. Genes marked with asterisk are used to represent the brain regions in the following results.

(C) Model network with all possible interactions between the brain region nodes and their reaction dependency on GSK3 activity. CT controls GSK3, which is self-activating to allow for steady-state GSK3 activity. During the topology selection, all undefined interactions were either activation or repression.

(D) Minimal optimised cost function value for all possible network topologies. Two optimal topologies with similar and overall lowest cost functions were identified.

(E) Best model as determined by the topology selection. The three brain regions formed a tristable switch, controlled by the level of GSK3, which is in turn controlled by CT concentration. Note that GSK3, MB and HB are self-activating to allow for respective constant steady state gene expression. Degradation of GSK3, FB, MB, HB not illustrated. F. Gene expression levels of the three brain region specific genes given by the experimental data (plain bars) and the model (striped bars) for varied concentrations of CT.
follows GSK3 activity when the latter is active at high levels. Furthermore, FB and MB are mutually repressive leading to a posterior limitation of the FB domain by the MB domain, recapitulating findings from in vivo studies, where an impairment of the MB domain led to a posterior expansion of the FB domain (Scholpp and Brand, 2003). For lower activity of GSK3, FB is no longer strongly expressed and can be fully repressed by the presence of MB or HB. This reduces the network to a co-repressive motif of MB and HB fate for lower GSK3 activity levels, which is controlled by their mutual repression strength and the repression through GSK3. In fact, the corresponding parameters were determined such that HB is repressing MB much stronger than vice-versa. GSK3’s repression on HB is even stronger compared to its repression of MB. It follows that for low GSK3 activity levels HB will dominate over MB and vice versa for higher GSK3 levels. This dynamic recapitulates the interactions occurring when the MB-HB boundary is induced, with MB and HB specific genes (Otx2, Gbx2) repressing each other (Brafman and Willert, 2017; Wittman et al., 2009). Additionally, Fgf8 expression in the MB-HB boundary is induced by HB and repressed by MB while upregulating HB and downregulating MB, leading to a nett asymmetrical repression pattern where HB represses MB more strongly than vice versa (Brafman and Willert, 2017; Wittman et al., 2009). In our minimal model this interaction via Fgf8 is encoded implicitly in the asymmetrical interaction between MB and HB. Moreover, the reduction of the tristable switch motif to a bistable motif for lower GSK3 activity levels indicates that the MB-HB boundary-like interactions are a central element of neural tube patterning.

Figure 1F shows the brain regions’ expression levels obtained from model simulations together with the experimental data used for the parameter optimisation. For most CT concentrations, model and data show high correlation. A significant deviation between model and data only occurred for the CT concentrations 0.8 μM and 1.0 μM. However, it is important to note that the overall structure of the brain regions’ response to varied CT concentration in this minimal model is close to the experimental data.

Sensitivity analysis of model parameters reveals key interactions

Next, we examined the sensitivity of the model output to changes of the model parameters to identify the key interactions. In vitro data were used as reference and consequently the results are given in terms of the cost function $E_c$, which was defined as the mean squared distance between model and data. Figures 2A and 2B show that the most sensitive rate constants are $c_4$, $c_9$, and $c_{12}$, which correspond to the self-activation of MB, HB and GSK3. A similar sensitivity pattern was found in the Hill coefficients $n_i$, for which also $n_4$, $n_9$, and $n_{12}$ were the most sensitive parameters, illustrating cooperativity and ultrasensitivity for MB, HB and GSK3. The most sensitive degradation rates were also the ones corresponding to the half-lives of MB, HB and GSK3 respectively ($\delta_2$, $\delta_3$ and $\delta_4$). This implied that the most sensitive part of the model was the balance between self-activation and inhibition of MB, HB and GSK3 activity and the resulting steady state gene expression level. This was to be expected, since those expression levels are controlling which node of the tristable switch is active. FB does not self-interact, and its expression is therefore strongly correlated to the activity of GSK3 at high GSK3 activity levels. Also, high GSK3 activity levels lead to repression of MB and HB, whereas at low GSK3 activity levels MB or HB repress the expression of FB, explaining the low sensitivity of the model to changes of the FB degradation rate $\delta_1$. The sensitivity of the repressions between FB and HB ($c_2$, $c_{10}$, $c_{11}$) was low, because either (at high GSK3 activity levels) HB was repressed by GSK3 or (at low GSK3 activity levels) FB was turned off. In both cases the sensitivities of the rate constants and Hill coefficients were low because the corresponding concentrations were close to zero. Another weak sensitivity was found in the repression of HB by MB ($c_9$, $n_9$), implying that the HB level was more dependent on its self-balance and repression by GSK3 than on repression by MB. Figure 2C shows the mean cost function change when all parameters were varied. We observed that the model was not sensitive to small variations of the model parameters. The mean cost function change for the variation of the whole parameter set of ± 10 % was similar to the maximum cost function change for the variation of an individual parameter, illustrating that the model is robust under the variation of parameters.

The sensitivity analysis showed that the key parameters of our model were the self-interactions of MB, HB and GSK3, since they not only controlled their own expression and activity level, but also which node of the tristable switch was active. Furthermore, the general dynamics of the model suggested that FB was proportional to GSK3, MB and HB were anti-proportional to GSK3, and the extent of the MB peak was controlled by the HB expression level. Following this reasoning, we formulated the hypothesis that knockdown of FB would not have a strong effect on the extent of the MB domain. However, knockdown of HB would remove the repression of MB for low GSK3 activity levels and would therefore lead to an extended MB region that includes the former HB region.
Knockdown and overexpression simulations showed that only HB knockdown increases the MB domain.

To test this hypothesis and to gain more insight into the transcriptional regulation of this patterning, we simulated knockdown (kd) and over-expression (oex) scenarios (Figure 2D). HB kd did not influence the interaction between FB and MB and lead to strong MB expression for CT > 0.2 μM, resulting in a more than five-fold larger CT window for MB fate. Knockdown of FB similarly did not influence the interaction between MB and HB and led to strong MB expression for CT < 0.3 μM. However, this only doubled the extent of the CT window for MB fate. Interestingly, when overexpressing MB, FB expression was lost, but the HB expression pattern was similar to wildtype. This gave rise to mixed MB-HB expression for higher CT concentrations. MB oex suppressed FB expression and lead to mixed MB/HB expression for higher CT concentrations. MB kd gave insight into the interaction between HB and FB and the double kd's highlight the reaction of the brain regions’ gene expressions to the CT concentration. Axes are the same for all panels, gene expressions are scaled between 0 and 1.

Figure 2. Sensitivity analysis of the model parameters and kd/oex predictions
(A) Fold-change of the cost function $\Delta E_i(\Delta p)$, with $\Delta p$ being a parameter set with one parameter varied between 0 and 10% relative to the optimised parameter set.
(B) Mean cost function change ($\Delta E_i(\Delta p)$) across $\Delta p = \pm 10\%$ relative to the optimised value.
(C) $\Delta E_i(\Delta p)$ for all parameters varied ± different relative amounts to the optimised parameter set.
(D) HB kd showed strong MB expression for CT > 0.2 μM. FB kd lead to strong MB expression for CT < 0.3 μM and wt behavior for higher CT concentrations. MB oex suppressed FB expression and lead to mixed MB/HB expression for higher CT concentrations. MB kd gave insight into the interaction between HB and FB and the double kd’s highlight the reaction of the brain regions’ gene expressions to the CT concentration. Axes are the same for all panels, gene expressions are scaled between 0 and 1.
found for low CT concentrations corresponds to a state that is not captured by our minimal model and we speculate that this state may be analogous to the multi-lineage priming state observed in other systems (Zhou et al., 2019). Knockdown of MB and HB illustrated that FB expression is negatively regulated by CT. Interestingly, the knockdown of FB and HB showed that MB reacts only weakly to CT at low levels. This implies that MB is only weakly regulated by CT itself. These results confirmed the findings from the parameter sensitivity analysis and suggest that protocols for the generation of DA MB neurons could be made more robust and independent of precise CT concentration by repressing HB fate. This would significantly increase the window of CT concentration that results in MB fate, while the repression of FB fate or the promotion of MB fate via overexpression would not lead to the same result.

Application of model to realistic geometry revealed dorsoventral stacking of rostrocaudal pattern

To further test the potential of the minimal rostrocaudal model, we merged it with the model of Balaskas et al. for dorsoventral patterning (Balaskas et al., 2012) and used the combined model to simulate the steady state pattern of the human neural tube in vivo. The combined model is shown in Figure 3 A. WNT signaling controls both dorsoventral and rostrocaudal patterning and therefore, the two model branches are linked through the WNT node. In the rostrocaudal network branch, a buffer node (U) translates the WNT signal into the GSK3-inhibition as achieved by CT in the in vitro case. On the dorsoventral network branch, Gli expression is repressed by WNT signaling and activated by SHH activity (Ulloa and Martí, 2009). Gli expression acts as selector for dorsoventral fate – like GSK3 in the rostrocaudal case – by activating the expression of ventral fate (Nkx2.2, V) and lateral fate (Olig2, L), which are mutually repressive. Both V and L repress the expression of dorsal fate (Pax6, D), resulting in a reduced tristable switch network motif.

We further investigated the role of the introduced U-node by analysing the sensitivity of the resulting pattern to changes of its associated parameters (Figure S2) and found that U self-activation and -repression exhibit

Figure 3. In silico patterning of the neural tube


(B) Three-dimensional model of neural tube geometry and the morphogen secretion sources. SHH (green): floor plate (fp) and zona limitans (zli); WNT (blue): roof plate (rp), the ventral midbrain (v) and isthmic organiser (io).

(C) Steady-state distribution of the patterned regions after applying the complete model. The geometry of the tube caused dorsoventral stacking of the rostrocaudal gene domains (* HB stacking, ** MB stacking).

(D) Rostrocaudal and dorsoventral steady-state pattern. Arrows indicate the direction of pattern establishment i.e. the main direction of morphogen action. Greyed areas in C and D are only shown for orientation and are not considered for pattern establishment. Dashed line indicates the position of the transversal section (x = 580µm), dot-dashed line indicates the position of the sagittal section (y = 80µm).
converse sensitivity to parameter changes effectively controlling the extent of the MB domain. Moreover, the pattern was more robust to changes of parameters associated with the modulation of U by WNT than to changes of parameters associated with the modulation of GSK3 by U, indicating that indeed the main function of U is buffering. A biological interpretation of this WNT-U-GSK3 cascade could be the dynamics of the β-catenin destruction complex (Stamos and Weis, 2013). In this scenario, U would correspond to the activity of the Frizzled receptor which sequesters the destruction complex and effectively reduces the rate of β-catenin degradation, which in our model is represented inversely by the GSK3 activity level.

To explore effects of the curved tube geometry and morphogen secretion sites on patterning, we set up a spatial simulation of the network on a realistic three-dimensional model of the rostral neural tube (de Bakker et al., 2016) (Figure 3B). The WNT signal originates from the roof plate (rp), the ventral midbrain (v) and the isthmic organizer (io) while SHH is secreted from the floor plate (fp) and the zona limitans intrathalamic (zl) (Carlson, 2013; Joksimovic et al., 2009; Prakash et al., 2006). The diffusion dynamics of both morphogens were estimated based on their respective protein structure (see STAR Methods).

The calculated steady state pattern (Figure 3C) agreed with previous studies for the dorsoventral branch (Balaskas et al., 2012) and also yielded the anticipated rostrocaudal pattern in the ventral half of the neural tube. Interestingly, in the dorsal half of the neural tube, the additional WNT signal from the roof plate lead to a stacking of the rostrocaudal brain regions in dorsoventral direction (* HB stacking, ** MB stacking in Figures 3C and 3D), which resulted in an L shaped MB and HB region in a sagittal cross section. Repeated simulations with different tube geometries and varied secretion location setups revealed that the roof plate signaling is vital to increase the extent of the midbrain region, especially in the bent tube geometry, and that this is mainly responsible for the observed stacking (Figures S3 and S4).

A frontal cross section revealed that, caudally, the stacked rostrocaudal pattern did not overlap with the dorsoventral pattern. The former was contained in the Pax6 regime, whereas the latter fell fully inside the FB region. This resulted in five distinct regions in dorsoventral direction and nine in total.

To verify our patterning results, we compared the expression pattern of dorsoventral markers with experimental data from (Balaskas et al., 2012), which consists of WT, Olig2−/−, Pax6−/− and (Olig2−/−, Pax6−/−) expression patterns from mouse embryos. We simulated the WT and the mutant conditions and calculated the relative extent of the expression domains in specific slices of our model via thresholding. Generally, we found that our model predictions and the data agreed well with an average absolute deviation of 8 ± 4% (Figure 4). A systematic trend across most conditions was an under-prediction of the V domain which was on average 8 ± 3% too small. Since this behavior was present even in the absence of D (Pax6−/−), it could be that either the SHH secretion rate or the rate of Gli induced V activation in our model was underestimated or that this mismatch is rooted in the physiological difference between developing mouse embryos and humans.

Overexpression simulations of morphogen secretions show high sensitivity of neural progenitor cell fate to morphogen levels

To investigate the influence of morphogen secretion levels, we simulated overexpression of SHH and WNT production. SSH oex did not affect the rostrocaudal pattern, but significantly changed the dorsoventral pattern (Figure 5A). The V domain was drastically dorsally enlarged compared to the wildtype (WT) and...
took up the whole ventral half of the neural tube. This led to a dorsal shift of the L domain, which, did not change in size. Consequently, the extent of the D domain was smaller. Through the dorsal shift of the pattern, the split of the dorsoventral domains occurred closer to the isthmic organiser and hence the extents of MB/HB + V/L domains were enlarged, leading to a decrease in size of the FB + L/V domains.

Overexpression of WNT had a small effect on dorsoventral patterning, decreasing the size of the V domain and shifting the L and D domains ventrally. However, the effects of this overexpression on the rostrocaudal pattern were more striking (Figure 5B). Most dominantly, the HB region was drastically enlarged, covering the whole caudal half of the neural tube and extending almost to the WT MB/FB boundary. This led to a ventral and caudal shift of the MB domain, which changed its characteristic L shape to a diagonal band and decreased its volume. Interestingly, through the dorsoventral stacking, the MB domain extended up to the caudal boundary of the neural tube. The FB domain was positioned in the ventral and rostral tip of the neural tube, covering less than half the volume of the WT FB domain. Combined, this led to a more pronounced dorsoventral stacking of the rostrocaudal brain regions in the caudal half of the neural tube, which gave rise to a large MB + L domain, while the volume of the WT HB + V domain was drastically reduced. Using the same quantification approach as for the comparison of the model with data from mouse embryos (Figure 5C), we found that the rostrocaudal pattern remained unchanged upon SHH oex. However, in the WNT oex condition the FB domain was absent and the HB domain was increased 11-fold. The MB domain was only enlarged by 3%, suggesting that the WNT expression level’s main effect on the MB domain is positional. The dorsoventral pattern shows a converse response to the two overexpression conditions, with the pattern being almost unchanged upon WNT oex. SHH oex leads to a three-fold enlargement of the V domain which reduces the D domain to half its normal size. Interestingly, we found that, analogous to the rostrocaudal pattern, the lateral domain’s size was unaffected by the overexpression (+1%).

Additionally, we simulated analogous knockdown (kd) conditions (Figure S5). We found that SHH kd does not affect the rostrocaudal pattern but abolishes the dorsoventral pattern, reducing it to only D expression and conversely, that WNT kd does not affect the dorsoventral pattern but reduces the rostrocaudal fate to only FB. This unsurprisingly illustrates the requirement of the morphogens for the establishment of the patterns.

**DISCUSSION**

We presented a simple mathematical model of rostrocaudal neural tube patterning. We determined its topology in an unbiased and data-driven fashion. The resulting configuration was that of a tristable switch of mutually repressing brain region fate under the control of the WNT target GSK3. Moreover, we showed that this configuration is not specific to a set of representative genes but is rather a general motif that was found to be conserved across different species.
for most region-specific genes, indicating a central role for this network motif in rostrocaudal patterning. The unbiasedly discovered gene regulatory network has at its core genetic toggle switches consisting of cross-repressing transcription factors, which are network motifs that were shown to control patterning at tissue levels (Davidson, 2010). The toggle switch motif has the capability of translating the continuous signal of a morphogen gradient into an on-off behavior, in our case WNT gradient signal into e.g. FB off/MB on. Our multiple toggle switch model was able to recapitulate data from in vitro studies on hPSCs cultured at different WNT signaling levels (Kirkeby and Parmar, 2012a, 2012b) and exhibited similar dynamics as recent experiments done on a synthetic in vitro setup (Rifes et al., 2020a; Rifes et al., 2020b). Since, the toggle switch motif can control the boundaries of gene expression domains (Balaskas et al., 2012; Briscoe et al., 2000), parameter perturbation or manipulation (e.g. via knockdown, overexpression) of one of the factors can lead to changes in the resulting pattern. For our network model parameter sensitivity analysis and in silico overexpression and knockdown experiments suggested that the repression of HB fate, rather than the repression of FB fate or the promotion of MB fate, is the most promising strategy to increase efficiency and robustness of DA MB generation protocols. Repression of HB increased the window of supplied GSK3 inhibitor CT that resulted in MB fate. It will be interesting to see if this result can be validated experimentally; one option could be to use synthetic neural tube patterning similar to the work recently published in (Rifes et al., 2020a; Rifes et al., 2020b).

To obtain an integrated model for the pattern of the neural tube, we used a ‘divide and conquer’ approach, combining models and data relating to different sub-processes of the full patterning. One major difficulty in the development of theoretical gene regulatory models of in vivo processes is a lack of suitable, quantitative data for parameter estimation and model validation. Here, we aimed to demonstrate that this difficulty can be overcome by adhering to the following strategy: (1) Division of the process of interest into distinct subprocesses. (2) Development of minimal models for each subprocess. (3) Re-integration of the subprocesses in a physiological context. Following this approach, we show that it can be sufficient to rely on quantitative data from in vitro experiments which, is more readily available, easier to obtain and ethically less controversial.

By combining our rostrocaudal model with a previously published model for dorsoventral neural tube patterning we obtained an integrated model for the pattern of the neural tube controlled by the morphogens SHH and WNT. On the rostrocaudal side of this model, a buffer node U, which translates WNT signal to GSK3 inhibition, needed to be introduced to achieve stable steady state rostrocaudal patterning. This node combined with the GSK3 node possibly corresponds to the dynamics of the β-catenin destruction complex as part of the WNT signaling cascade and the need for it is an example for the dynamic difference between signaling cascades and direct modulation of gene expression. It should be noted that the configuration of the rostrocaudal branch of the integrated network is very similar to the dorsoventral branch, with both branches having a morphogen level-regulated multiple toggle switch configuration at their core. This is very much in line with the idea that network motifs like feedback and mutual repression predominate parts of the modular structure of gene regulatory networks (Alon, 2007; Davidson, 2010). To test the capabilities of the combined model, we simulated the patterning of the early human neural tube. For this, we set up a realistic three-dimensional model of the neural tube, which included the major morphogen secretion sites. The diffusion of the morphogens from these sites led to stable patterning of the tube into distinct regions, which are similar to existing data. However, we found that, in our model, the isthmic organiser (the posterior WNT secretion site) and the MB-HB boundary did not co-localise, with the latter being shifted anteriorly. This mismatch is most likely due to our model lacking of dynamic, brain region specific, auto-regulation of the WNT response during the induction of the MB-HB boundary as indicated in (Brafman and Willert, 2017). The integration of this sub-process into our model represents a promising next step for the expansion of the model. Interestingly, the bent geometry of the neural tube, combined with WNT secretion from the roof plate led to dorsoventral stacking of the rostrocaudal domains in the rostral half of the tube. Repeated simulations with different tube geometries and varied presences of the morphogen sources showed that roof plate signaling is mainly regulating the extent of the midbrain region and the dorsoventral stacking phenomenon. Unfortunately, no data was available to validate these model predictions. It would therefore be very interesting to find out if this is a shortcoming of the model or indeed a patterning mechanism. Data for such validation could be obtained for example by live microscopy of the neural tube in zebrafish embryos with fluorescently labeled region-specific genes. Lastly, we simulated the overexpression of morphogen secretion, which illustrated that cell fate and consequently neural tube patterning is sensitive to the abundance of morphogens seen by individual cells. In the WNT overexpression case, the model predicted an increase in HB fate, which is consistent with several previous studies.
SHH overexpression resulted in a drastic enlargement of the V-domain, shifting of the C-domain and size reduction of the D-domain, which is consistent with findings in (Jeong, 2004). Moreover, we find that the general sensitivity of neural progenitor cells to the abundance of WNT and SHH ligands predicted by the model to be in line with a recent study on hPSCs (Strano et al., 2020), implying that the secretion and distribution of morphogen ligands in a developing embryo have to be precisely and robustly regulated.

In summary, our 3D computational model demonstrates how the combination of sub-process models can be used to modularly construct a modeling framework leading to better understanding of complex and inaccessible biological processes. Moreover, the presented model for rostrocaudal neural tube patterning can, despite its simplicity, recapitulate the main features of neural tube patterning and neural differentiation in dependence of WNT signaling and predict strategies of improving the efficiency of DA MB generation protocols. In the future, targeted in vitro experiments are required to test the predictions of this model. Therefore, this study is only a first step toward an integrated and conclusive view for the 3D patterning of the neural tube in vivo.

Limitations of the study

It is important to note that the identification of gene expression clusters via hierarchical agglomeration is a correlative method. This means that the three identified clusters do not necessarily have to be connected mechanistically. Specifically, we can make no statement about whether the selected representative genes are interacting directly. Moreover, we noticed discrepancies between our minimal model and the used qPCR data for some concentrations of CT. This is most likely due to the simplicity of our model. However, the general dynamic of our model fits well with the data. Furthermore, the results of the integrated three-dimensional model could not be rigorously validated due to a lack of available data. Moreover, neural tube patterning is a dynamic process, yet our minimal 3D model only recapitulates an already patterned state in a static fashion. This means that cells can only receive signals from pre-defined secretion sites instead of being able to dynamically feedback and modulate the strength of morphogen secretion. Therefore, the model does not account for the dynamic induction of morphogen expression sites throughout development, such as the establishment of the MB/HB boundary.

STAR METHODS

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SUPPLEMENTAL INFORMATION

Supplemental information can be found online at https://doi.org/10.1016/j.isci.2021.102559.

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**AUTHOR CONTRIBUTIONS**

MB, AE, VO designed the study. MB, AE, VO wrote the manuscript. MB built the rostro-caudal model, conducted computational analysis. AE built the 3D computational model. MP, AK, JD-O, SN provided the experimental data. JD-O, SN explicated and conceptualised the use of experimental data. All authors provided inputs and comments on the manuscript.

**DECLARATION OF INTERESTS**

The authors declare no competing interests.

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**REFERENCES**


Kirkeby, A., and Parmar, M. (2012a). Building authentic midbrain dopaminergic neurons from...


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KEY RESOURCES TABLE

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RESOURCE AVAILABILITY

Lead contact
Further information and requests for resources and reagents should be directed to and will be fulfilled by the Lead Contact, Victor Olariu (victor@thep.lu.se).

Materials availability
This study did not generate new unique reagents.

Data and code availability
The used qPCR data and the code generated during this study are available at https://github.com/max-brambach/neural_tube_patterning_paper.

METHOD DETAILS

Clustering of gene expression data
For a gene with expression level $x$ the normalisation was chosen such that $R = \frac{x}{\bar{x}}$ with the normalised gene expression $R$, the mean gene expression $\bar{x}$ across the different CT levels and the corresponding standard deviation $\sigma_x$.

The normalised gene expression data was clustered using hierarchical agglomerative clustering (Mullner, 2011). As method for the computation of the cluster distance, the Nearest Point Algorithm was used, meaning that the minimal distance between two clusters was considered as their distance. The used metric for the determination of the distance was the Euclidean distance.

Optimisation of model towards in vitro data
The parameters of the model were optimised using the experimental data. For the purpose of parameter optimisation, the expression of each brain region’s specific genes was normalised such that its maximum value was 1 via division of all values by the maximum value. During the optimisation, the network was initialised with $FB = MB = HB = GS = 1$ for all used CT concentrations. The evolution of the gene expressions was computed iteratively until the steady state was reached. This steady state gene expression for a specific
CT level was considered as the model output. The cost function $E_d$ measures the deviation of the model output $r$ from the data $d$ and is computed using

$$E_d(p) = \sum_i \sum_j (d_{ij} - r_i(p))^2$$

with the first sum going over the different CT concentrations, the second sum going over is \{FB, MB, HB\} and the parameter set $p$. An optimal set of parameters is found by minimising $E_d(p)$ with respect to $p$ using a L-BFGS-B algorithm (Byrd et al., 1995). The parameter set used in this article is shown in the table below.

### Similarity of model topologies

The similarity of different model topologies (Figure S1B) was quantified using a topology score defined as the number of identical interactions normalised to the total number of interactions of two model topologies. I.e. the topology score is zero for all interactions being different and one for identical topologies.

### Differential equations

The set of differential equations describing the in vitro model mathematically was constructed using the Hill formalism and resulted in

$$\frac{d\{FB\}}{dt} = \frac{c_1[\text{GSK3}]^{n_1}}{1 + c_1[\text{GSK3}]^{n_1} + c_2[\text{MB}]^{n_2} + c_3[\text{HB}]^{n_3}} - \delta_1[\text{FB}]$$

$$\frac{d\{MB\}}{dt} = \frac{c_4[\text{MB}]^{n_4}}{1 + c_4[\text{MB}]^{n_4} + c_5[\text{FB}]^{n_5} + c_6[\text{HB}]^{n_6} + c_7[\text{GSK3}]^{n_7}} - \delta_2[\text{MB}]$$

$$\frac{d\{HB\}}{dt} = \frac{c_9[\text{HB}]^{n_9}}{1 + c_9[\text{HB}]^{n_9} + c_10[\text{FB}]^{n_{10}} + c_11[\text{MB}]^{n_{11}} + c_12[\text{GSK3}]^{n_{12}}} - \delta_3[\text{HB}]$$

$$\frac{d\{\text{GSK3}\}}{dt} = \frac{c_{12}[\text{GSK3}]^{n_{12}}}{1 + c_{12}[\text{GSK3}]^{n_{12}} + c_{13}\{\text{CT}\}^{n_{13}}} - \delta_4[\text{GSK3}]$$

$$\frac{d\{\text{CT}\}}{dt} = 0$$

The set of differential equations defining the in vivo model are

$$\frac{d\{P\}}{dt} = \frac{\alpha}{1 + \left(\frac{[N]}{N_{\text{crit}}}\right)^{n_1} + \left(\frac{[O]}{O_{\text{crit}}}\right)^{n_2}} - k_1[P]$$

$$\frac{d\{O\}}{dt} = \frac{\beta[G]}{1 + [G]^{n_3}} - k_2[O]$$

$$\frac{d\{N\}}{dt} = \frac{\gamma[G]}{1 + [G]^{n_3}} - k_2[N]$$

$$\frac{d\{\text{GSK3}\}}{dt} = \frac{c_{12}[\text{GSK3}]^{n_{12}}}{1 + c_{12}[\text{GSK3}]^{n_{12}} + c_{13}[U]^{n_{13}}} - \delta_4[\text{GSK3}]$$

$$\frac{d\{U\}}{dt} = \frac{c_{14}[\text{WNT}]^{n_4} + c_{15}[U]^{n_5}}{1 + c_{14}[\text{WNT}]^{n_4} + c_{15}[U]^{n_5}} - \delta_5[U]$$

$$\frac{d\{G\}}{dt} = \frac{\delta[\text{SHH}]}{1 + \left(\frac{[\text{WNT}]}{W_{\text{crit}}}\right)^{n_6}} - k_4[G]$$

$$\frac{d\{\text{WNT}\}}{dt} = D_{\text{WNT}}[\text{WNT}] - \delta_{\text{WNT}}[\text{WNT}]$$

$$\frac{d\{\text{SHH}\}}{dt} = D_{\text{SHH}}[\text{SHH}] - \delta_{\text{SHH}}[\text{SHH}]$$
The self-activation term of FB used during the model selection is not shown in the equations above, since it is not used after this step. The term was implemented in the ODE for FB expression following the Hill formalism, i.e. in the denominator for repression and in both numerator and denominator for activation.

The morphogen diffusion of the in vivo model was implemented using the discrete version of Fick’s law

$$\frac{d[X_i]}{d[t]} = D \sum_{\text{Neighbours}} [X_j] - [X_i]$$

with the index of the current cell $i$, the diffusion constant $D$, and $[X]$ being the concentration of either WNT or SHH. For each time step, the morphogen gradient pattern was updated prior to the intra-cellular network. The model reaches a steady state pattern, as shown in Figure 3C.

**Model parameters and initial conditions:**

The model parameters are summarized in the following table. Unlisted parameters of the dorsoventral model are listed in (Balaskas et al., 2012). During the model selection, the FB self-interaction parameters of the optimal topologies were $c_0 = 0.0005$ and $n_0 = 1$.

For the in vitro simulations, the system was initialised with $FB = MB = HB = GSK3 = 1$. The 3D in vivo simulations were initialised with $WNT = SHH = U = P = O = N = 0$, $FB = GSK3 = 1$, $MB = HB = 0.001$, $G = 3$. Morphogen producing cells were held constant at $WNT_{\text{prod}} = 2$, $SHH_{\text{prod}} = 1$.

**Kd and oex implementation**

The simulation of knockdown and overexpression in vitro was achieved by fixing the respective kd/oex node’s derivative to 0. The initial expression of the node then determined its behaviour, with kd being simulated by $\frac{1}{c_i}$ and oex by $\frac{1}{c_i}$. The morphogen secretion overexpression in vivo was implemented by increasing the morphogen level of the secreting cells ten-fold. In all cases, the steady state expression pattern is considered the model output.

**Morphogen diffusivity**

The morphogens’ diffusion coefficients $D_{WNT}$, $D_{SHH}$ were estimated following a method proposed by He and Niemeyer based on the radius of gyration $R_G$ of the protein (He and Niemeyer, 2003). $R_G$ was estimated according to (Hong and Lei, 2009) for physiological conditions:

$$R_G = 3N^\frac{2}{3} \text{Å}$$

with $N$ being the protein chain length (number of amino acids). Inserting the protein lengths $N_{WNT} = 370$ and $N_{SHH} = 462$ (UniProt Consortium, 2018) yields $R_{WNT} \approx 32 \text{Å} = 3.2 \text{nm}$ and $R_{SHH} \approx 35 \text{Å} = 3.5 \text{nm}$.

Subsequently, we applied the estimate

$$D = \frac{6.85 \times 10^{-15} \text{T}}{\eta \cdot \sqrt{M^b \cdot R_G}}$$
with $D$ in units of $\text{m}^2\text{s}^{-1}$, temperature $T = 310\text{K}$, viscosity $\eta = 0.75 \text{cP}$ (Puchkov, 2013) and the molecular Mass $M (M_{\text{WNT}} = 40.98\text{kDa}, M_{\text{SHH}} = 49.61\text{kDa})$ in $\text{kg} \cdot \text{kmol}^{-1}$, yielding

$$D_{\text{WNT}} = 150.7 \mu\text{m}^2\text{s}^{-1} \text{ and } D_{\text{SHH}} = 133.4 \mu\text{m}^2\text{s}^{-1}.$$  

**Quantification of gene expression**

Gene expression on a tube slice was quantified by calculating percentage $p_{\text{gene}}$ of the slice area where the gene expression is higher than a threshold $T$:

$$p_{\text{gene}} = \frac{A_{\text{gene}>T}}{A_{\text{Total}}}$$

where $A_{\text{gene}>T}$ is the area where the gene expression is larger than the threshold and $A_{\text{Total}}$ is the area of the entire slice. Since strength of expression varies for the rostrocaudal and the dorsoventral network branch, the threshold was set to $T=1$ for the dorsoventral branch and to $T=0$ for the rostrocaudal branch.

**Computational methods**

The \textit{in vitro} model equations were solved numerically using a fourth order Runge-Kutta algorithm with temporal step size $h = 2$. The equations of the \textit{in vivo} model were solved using the explicit Euler method.

All computational work was performed in Python 3.7 with the extensions NumPy (Harris et al., 2020), SciPy (Virtanen et al., 2020), Matplotlib (Hunter, 2007), Pandas (McKinney, 2010; Pandas Development Team, 2020) and seaborn (Waskom, 2021). The neural tube model and the sources of morphogen secretion were set up in MagicVoxel, an open source voxel editor software. Cells were approximated as cubes with side length 10$\mu\text{m}$ with the morphogen secretions sites positioned as illustrated in Figure 3B.

**QUANTIFICATION AND STATISTICAL ANALYSIS**

All quantification and analyses were performed as described in the methods details and computational analyses sections of the STAR Methods. Data are presented as mean ± standard deviation.